

(43) Date of A Publication **23.01.2002**

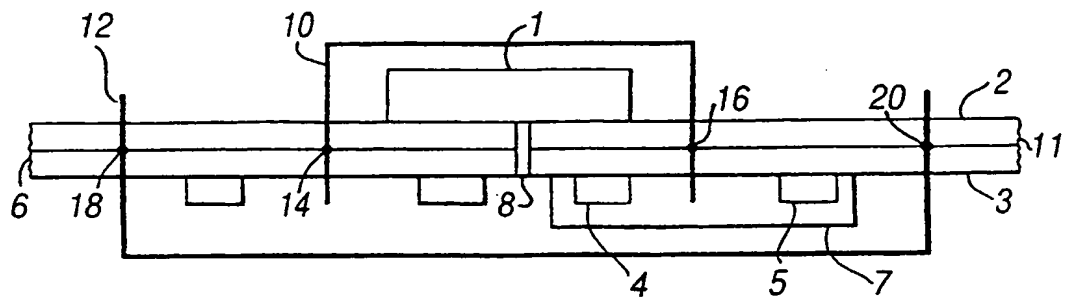


Fig. 1

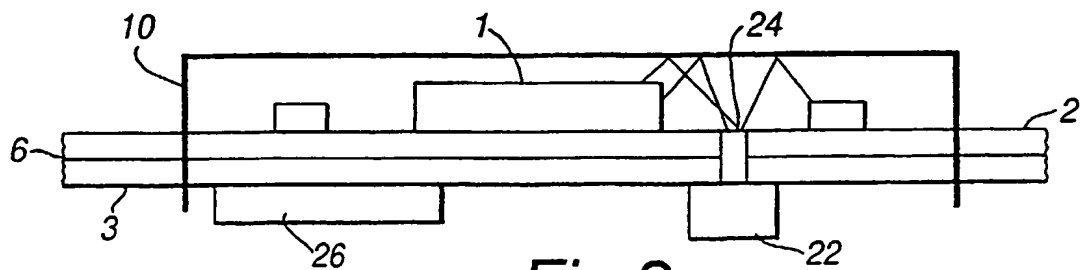


Fig. 2

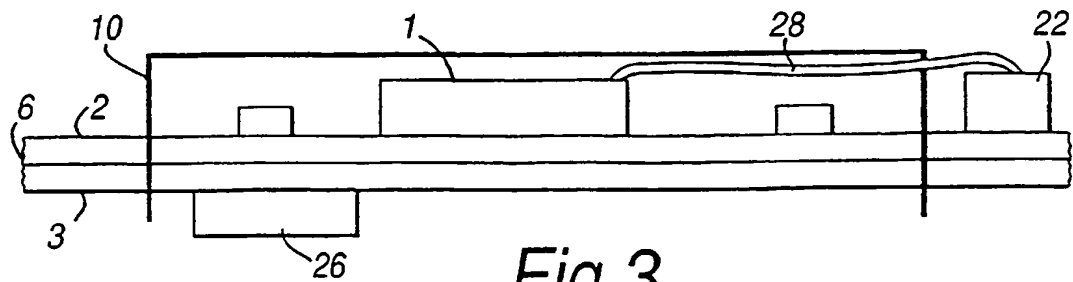


Fig. 3

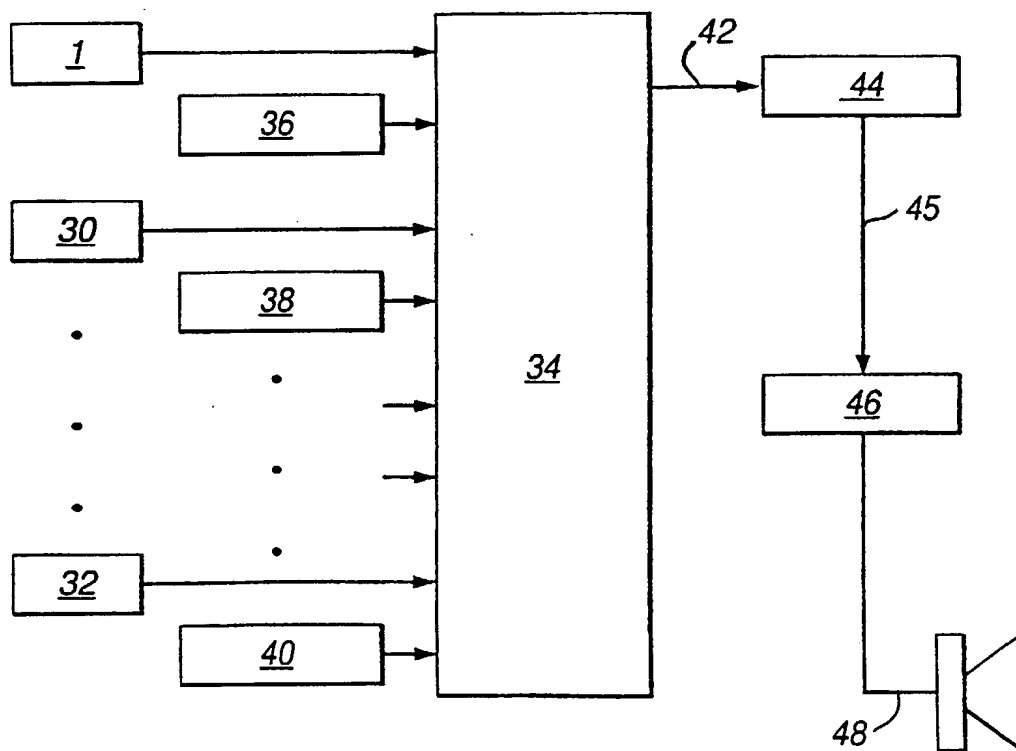


Fig.4

**IMPROVEMENTS IN OR RELATING TO
PERSONAL RADIATION DOSEMETERS (DIV1)**

The present invention relates to personal radiation doseimeters or indicators which operate to measure radioactivity doses to which personnel are exposed.

Electronic personal doseimeters are worn by personnel in potentially hazardous environments. An example of such an environment is a nuclear power station where there is the possibility, however small, of personnel receiving radiation doses which may be potentially hazardous to their health. For this reason, personnel are often required to carry or wear an electronic personal doseimeter which operates to detect radiation and provide an indication of an amount of radiation to which the personnel are exposed at any time.

Electronic personal doseimeters are provided with radiation detectors which operate to generate a signal for each particle of radiation detected. Electronic personal doseimeters may furthermore provided with a means for converting signals generated or detected by the radiation detector into an audio signal so that a person wearing the doseimeter is given an audible indication of a current level of radiation to which their body is being exposed.

Typically, during a day's activity, a person working in a power station may be in an environment where there are relatively large amounts of radiation during one part of the day, and in an environment in which there is virtually no radiation, or

only background radiation present, in another part of the day. As such, a technical problem exists in that, if the electronic personal detector worn by a person should malfunction at a time when the person is in an environment where there is no radiation, then the person wearing the detector will not be alerted to the presence of harmful amounts of radiation as a result of the malfunction of the dosimeter. A technical problem therefore exists in arranging for the radiation dosimeter to be tested in a way which provides regular confirmation of the integrity of the radiation dosimeter.

The technical problem of testing and confirming the integrity of a radiation dosimeter is addressed by the present invention.

According to the present invention, there is provided a personal radiation dosimeter comprising a radiation detector means coupled to an electronic measurement circuit arranged in combination therewith to generate signals representative of an amount of radiation detected by said radiation detector, wherein said radiation detector means is provided with a light source optically coupled to said radiation detector and arranged to operate under control of a test control circuit to generate light of a wavelength which may be detected by said radiation detector, thereby providing in combination with said electronic measurement circuit an integrity test for said radiation detector means.

The term light as used herein refers to light in both the visible and invisible spectra.

By arranging for the electronic personal dosimeter to be provided with a light source capable of generating photons in the

visible or infra-red spectra, and arranging for the test control circuit to generate or energise the light source at predetermined intervals, the electronic personal dosimeter is provided with a means for testing the integrity of the radiation detector and the electronic circuit means thereby confirming the integrity of the radiation dosimeter.

The light source may be a light emitting diode. The optical coupling may include a fibre optic. The optical coupling may be effected from reflection from a surface of the shield.

A further problem with known electronic personal dosimeters is that the radiation detectors are susceptible of providing false readings as a result of electromagnetic interference. For example, stray electromagnetic fields generated by computer monitors, radar systems or mobile phones may cause a false reading of a radiation particle to be detected.

The radiation detector should also be provided with a screen or shield from certain low energy X-rays or gamma photons in order to filter such low energy X-rays or gamma photons in order to provide a better representation of radiation received by the human body. To this end, the radiation detector must be provided with a radiological shield as well as a shield from electromagnetic interference. A technical problem therefore exists in providing a personal radiation dosimeter with a shield from both electromagnetic interference and a radiological shield. This technical problem is addressed by a first aspect of the present invention.

According to a first aspect of the invention there is provided a personal radiation dosimeter comprising a radiation detector means coupled to an electronic measurement circuit and arranged in combination to generate signals representative of an amount of radiation received by said radiation detector means, wherein there is further provided a shield arranged to be electrically coupled to an earth plane and to substantially surround a volume in which said radiation detector means is disposed, said shield being fabricated from electrically conductive material so as to provide substantial electromagnetic screening and said electrically conductive material has a composition and density which is sufficiently high to provide substantial radiological shielding for substantially low energy radiation particles, said shield being thereby arranged to provide both electromagnetic and radiological screening.

The electrically conductive material may be a metal. The metal may be tin. The metal may be an alloy such as pewter.

By fabricating a shield which provides both radiological and electromagnetic screening to the radiation detector, a reduction in size and weight of the radiation dosimeter may be effected. This is particularly advantageous for personal dosimeters.

Known radiation dosimeters are arranged to provide an audible signal for an integral number of particles of radiation detected by a radiation detector. However, there is a requirement to provide instruments to detect radiation, with different characteristics. This requires the use of more than one detector, each of which is arranged to detect radiation with different

characteristics. A technical problem therefore exists in providing an audible signal which is representative of the radiation dose rate received by the human body without dependence upon the characteristics of the radiation detector.

Known radiation dose rate meters use a microprocessor to effect processing and combination of signals from a plurality of detectors. However, microprocessors consume a significant amount of power whilst in an operating mode and for this reason may be only activated on a basis of a duty cycle. The duty cycle has an effect that battery power is economised. However the duty cycle of the microprocessor is such that a maximum repetition frequency of the audio signal indicative of the radiation dose rate may be unacceptably low. These technical problems are addressed by a second aspect of the present invention.

According to a second aspect of the present invention there is provided a personal radiation dosimeter for generating a monitor signal representative of a radiation dose rate, said radiation dosimeter comprising a radiation detector means coupled to an electronic measurement circuit arranged in combination therewith to generate signals representative of an amount of radiation received by said radiation detector, wherein said electronic measurement circuit includes at least one data store, an accumulator means and control circuit means, which control circuit means is coupled to said radiation detector means and arranged to add a predetermined number stored in said data store to an accumulated total stored in said accumulator in response to signals from said radiation detector means, said

control circuit being arranged to generate a monitor signal for each increment of said accumulated total by said predetermined numerical threshold, which monitor signal is fed to an audio signal generator so as to provide an audible signal in accordance with said increment, a repetition frequency of said audible signal being thereby representative of said radiation dose.

By arranging for a control circuit to add a predetermined number to an accumulator means when a signal is received from the radiation detector means, a scaling of the signal received or generated by the radiation detector means may be effected by appropriately selecting the number stored in the data store and the numerical threshold which is used to trigger the monitor signal when the numerical threshold is reached. In this way scaling of the signal generated by the radiation detector means is effected without a requirement for a microprocessor, thereby allowing the control circuit to be implemented in hardware thus effecting a substantial improvement in power consumption of the electronic personal dosimeter.

The personal dosimeter may further include at least one other radiation detector means and at least one other data store wherein said at least one other data store includes a further predetermined number and said control circuit operates to add said further predetermined number to said accumulator on consequent upon receipt of signals from said at least one other radiation detector means.

By providing a further radiation detector which may be arranged to detect a different type or energy of radiation particle

and providing a further data store which is arranged to be pre-stored with a further predetermined number, the control circuit may be arranged to add said further predetermined number when said further radiation detector means detects the presence of radiation. In this way the accumulator maintains a total representative of an amount of radiation detected by said radiation detector means and said further radiation detector means in proportion to the first and further predetermined numbers. By selecting the first and the further predetermined numbers independently upon the numerical threshold, the radiation dosimeter may be arranged to generate a monitor signal at a repetition frequency which is arranged to provide an audible indication determined by the relative amounts and harmful effect of the radiation detected by the first and further radiation detector means.

One embodiment of the present invention will now be described by way of example only with reference to the accompanying drawings wherein:-

Figure 1 is a schematic block diagram of a personal radiation dosimeter illustrating, in particular, a screen arrangement around the radiation meter,

Figure 2 is a schematic block diagram of part of the personal radiation meter shown in Figure 1 illustrating operation of a means for testing the radiation detector shown in Figure 1,

Figure 3 is a schematic block diagram of part of the personal radiation dosimeter shown in Figure 1 showing a further arrangement for testing the radiation detector, and

Figure 4 is a schematic block diagram of an arrangement for generating an audible monitor signal in accordance with the detected radiation by the radiation detector means.

Part of an electronic radiation dosimeter is illustrated in a block diagram form shown in Figure 1. In particular, Figure 1 has been provided to illustrate an arrangement for forming a shield for the personal radiation dosimeter so as to provide protection from both electromagnetic interference and from low energy radiation particles.

In Figure 1 a radiation detector 1, is shown to be disposed on a first plane 2 of a printed circuit board 11. On a second plane 3 of the printed circuit board, there is also shown further electronic components 4, 5, disposed upon the second plane 3. Interposed between the first and second planes 2 and 3 of the printed circuit boards, is a ground or earth plane 6, which is fabricated from a suitable material such that electrical conductivity is provided along its length. Also shown in Figure 1 is an electrical via 8, for providing a means for electrically coupling the radiation detector 1, to components on the second plane 3 of the printed circuit board 11. As will be appreciated, the printed circuit board 11 may be provided with a plurality of layers which may be electrically connected using conventional technology known to those skilled in the art. Furthermore the physical arrangement of the electronic components 4, 5, within an enclosure provided by the shield may be different to that shown in Figure 1, and many other arrangements may be envisaged.

In operation an electronic personal radiation dosimeter detects radioactive particles or high energy X-ray emissions using the radiation detector 1, which serves to generate a signal indicative of the presence of such a radiation particle. Such signals are thereafter fed to an electronic measurement circuit which is made up from components 4, 5, disposed on the printed circuit board 3. Since the radiation detector 1, is arranged to detect the presence of radiation particles and high energy photons, the radiation detector 1, must be shielded from other extraneous radiation such as electromagnetic interference or other electrical signals. This protection is further enhanced by disposing the earth or ground plane 6 interposed between the first and second planes 2, 3 of the circuit board.

Electronic personal radiation dosimeters are arranged to provide an indication of an amount of radiation absorbed by the body. As such, it is necessary to provide the radiation detector 1 with an amount of shielding sufficient to attenuate low energy radiation particles or X-ray photons so that radiation detected by the radiation detector is a more accurate representation of a total amount of energy received by the human body. Hence it is necessary to provide a shield, known as a radiological shield, to prevent low energy radioactive particles from being detected by radiation detector 1. The shielding should be arranged to provide substantially 360° of shielding of the radiation detector 1.

As aforementioned, electronic radiation dosimeters are also sensitive to electromagnetic interference. Examples of sources of such electromagnetic interference are stray electromagnetic fields

from monitors or from radar equipment which by its nature transmits high energy electromagnetic pulses, or from mobile telecommunications equipment providing interference at microwave frequencies. It is therefore necessary to provide both electromagnetic and radiological screening to an electronic radiation dosimeter. Figure 1 provides an illustration of an arrangement of such a screen. In Figure 1 a shield is provided in a first part 10, and a second part 12. The first part 10, is arranged to provide a screened volume around the radiation detector 1. The shield first part 10, is arranged to be electrically coupled to the earth plane 6, at a plurality of conveniently located fixing points. An example of such fixing points is shown in Figure 1 either side of shield first part 10 at points 14, 16.

The second part of the screen 12, is also electrically coupled to the earth plane 6, at points 18, 20. The second part of the shield 12, is arranged to provide a screened volume for the electronic components 4, 5, of the electronic measurement circuit 7, disposed on the second printed circuit board 3. By electrically connecting the first and second parts of the shield 10, 12, to the earth plane, the radiation detector and electronic components 4, 5, are provided with an electromagnetic shield in the form of a "Faraday cage". The first and second parts of the shield 10, 12, are arranged to provide substantially 360° of screening such that there is no line of sight for any radiation particles to the detector 1. As will be appreciated by the cogniscenti, the shield 10, 12, can also be fabricated in other arrangements.

By fabricating the first and second parts of the shield from a material which is both conductive and provides an appropriate attenuation of low energy radiation particles or low energy X-ray photons, the shield 10, 12, may provide radiological shielding as well as electromagnetic interference shielding. An example of such a material may be a metal such as tin. Tin may provide appropriate conductivity to effect electromagnetic interference shielding, whilst having an atomic number which is sufficiently high to attenuate low energy radiation particles before reaching the radiation detector 1. Another example of such a material is zinc. A further example is to use an alloy such as pewter which combines copper and tin so that appropriate levels of radiological shielding are effected whilst maintaining appropriate electromagnetic interference shielding. Pewter has the further advantage of being mechanically workable so that the first and second parts of the shield 10, 12, may be formed, and has a melting point which is higher than that of conventional solder. As such, the shield 10, 12, may be suitably shaped and formed in components and soldered using standard circuit assembly techniques.

In use, electronic personal radiation doseimeters, are worn by personnel in potentially hazardous environments such as nuclear power stations. As such an amount of radiation detected by such a doseimeter will vary throughout daily use in accordance with an environment in which the personnel are present. For this reason, there may be periods during a day in which the personnel are exposed to little or no radiation. However, equally the

personnel may be situated in environments where there are potentially hazardous levels of radiation. If a situation were to occur wherein the personal radiation dosimeter were to malfunction in an environment in which little or no radiation is present, then personnel may be subjected to hazardous levels of radiation without being alerted to this danger. To effect a remedy to undetected malfunctions of the personal radiation meter, a regular and frequent automatic self-test facility is provided. Although testing of the electronic measurement circuit may be effected using a known arrangement of coupling test signals into amplifiers and other electronic components of the measurement circuit, such test circuits would not provide a suitable test for the integrity of the radiation detector 1. An example of a radiation detector 1, is a photo sensitive detector which is arranged to detect ionising radiation. Such radiation detectors may also detect longer wavelength photons of light in the visible or infra-red spectra and it is for this reason that the radiation detector 1, must be screened from ambient light for correct operation.

An embodiment of the present invention illustrated in Figure 2 shows a means for providing a test for the integrity of the radiation detector 1. Figure 2 provides a schematic block diagram of part of the electronic personal radiation dosimeter shown in Figure 1 where parts also appearing in Figure 1 bear identical numerical designations. In Figure 2 a light emitting diode 22, is disposed on the second plane 3 of the printed circuit board. In the first and second planes of the printed circuit board and the earth plane 6, there is provided a through hole 24, for

communicating light generated by the light emitting diode 22, into the volume shielded by the first part of the shield 10. Also coupled to the light emitting diode 22, is a test circuit controller 26. The test circuit controller 26, is arranged to be as far as possible electrically isolated from other components of the electronic measurement circuit 7, such that there is no electrical coupling of signals from the test circuit controller 26, to the electronic measurement circuit 7.

In operation the test circuit controller 26, operates to control the light emitting diode 22, so as to provide a regular and frequent test of the integrity of the radiation detector 1 in combination with the electronic measurement circuit 7. The test circuit controller 26, operates to excite the light emitting diode 22, thereby generating photons of light which have a wavelength sufficient to cause detection of such photons by the radiation detector 1. The photons pass through the through hole 24 into the volume in which the radiation detector 1 is situated. Photons may reach the radiation detector indirectly via reflection from the inside surface of the first part of the shield 10. An alternative arrangement is illustrated in Figure 3 where parts also appearing in Figures 1 and 2 bear identical numerical designations. In Figure 3 a fibre-optic 28, is provided to effect optical communication of photons generated by the light emitting diode 22, to the radiation detector 1. As will be appreciated by those skilled in the art, other means may be provided to effect optical coupling of the light generated by the light emitting diode 22 to the radiation detector 1.

Electronic personal radiation dosimeters are also provided with a means for providing an audible monitor signal which alerts the carrier of the personal radiation dosimeter to the presence of radiation. An example of such an arrangement is an audio signal generator coupled to the measurement circuit and arranged to generate an impulse of sound or 'chirp' in accordance with radiation detected by the radiation detector 1. In this way the frequency of the impulses or chirps is arranged to be in proportion with the current quantity of radiation detected by the radiation detector 1.

As is known to those skilled in the art, there are various types of radiation particle. Each type of radiation particle may furthermore have a substantial range of energy. As such, different radiation detectors may be required to detect each of these types or energies of radiation. For this reason, the personal radiation dosimeter may be provided with a plurality of detectors, each of which is arranged to detect radiation particles with particular characteristics. The effect of a particle of radiation detected by the radiation detector for a low energy particle and radiation particle detected by the radiation detector for high energy particles are required to be scaled in accordance with difference in the harmful effects on the human body. After scaling, the personal radiation dosimeter must be arranged such that a repetition frequency of the audible monitoring signal is adjusted in accordance with the characteristics and quantity of radiation detected by each radiation detector.

A schematic block diagram of an arrangement which serves to generate such an audible monitoring signal is shown in Figure 4. In Figure 4 three radiation detectors 1, 30, 32 are shown to be connected to an audible monitor control circuit 34. Also connected to the audible monitor control circuit 34 are three data stores 36, 38 and 40. Connected to an output 42 of the audible monitor circuit controller 34 is an accumulator 44. Connected to an output of the accumulator 44, is an audible signal generator 46. Connected to an output of the audible signal generator 46, is a loud speaker 48. The loud speaker 48, may for example be a piezo buzzer. Although the audible signal generator 46 shown in Figure 4 has been illustrated with three radiation detectors 1, 30, 32, it will be readily appreciated by those skilled in the art that a number of radiation detectors may be provided, each of which is arranged to detect a predetermined or predefined type of radiation particle. Associated with each of the radiation detectors 1, 30, 32 is one of three data stores 36, 38, 40. Each of the data stores 36, 38, 40, is arranged to store a predetermined number representative of a typical dose delivered to the human body by a radiation particle detected by the corresponding radiation detector. In operation, the monitor circuit controller 34, operates to add the predetermined numbers stored in the data stores 36, 38, 40, into the accumulator 44, consequent upon receipt of a signals from the corresponding radiation detector 1, 30, 32, indicative of a detected particle of radiation. Thus, if for example radiation detector 1, detects a radiation particle, then the predetermined number stored in data store 36, is added to the

running total in accumulator 44. When the accumulated total contained in accumulator 44, reaches a predefined numerical threshold, a signal is generated on conductor 45, representative of a predetermined amount of radiation energy received by the radiation detector. The signal fed on conductor 45, from accumulator 44, is received by the audible signal generator 46, which operates to generate a sound impulse or chirp fed to the loudspeaker 48, for audible conveyance of the detected quantity of radiation. The predefined numerical threshold in combination with the predetermined numerical values in the data stores 36, 38, 40 are arranged to generate a monitoring signal with a repetition frequency in proportion to the current dose rate from radiation particles received by the radiation dosimeter. Once the monitor signal has been generated, the running total in accumulator 44 is reduced by the predefined numerical threshold, after which the aforementioned adding of the predetermined numbers to the accumulator 44, continues. One way of effecting this reduction is to set the aforementioned predetermined numbers so that the predefined numerical threshold is the maximum value of the accumulator. The monitor signal may then be generated from the accumulator 44, by simply an overflow indicator. However, as will be readily appreciated by those skilled in the art, other means may be used in order to effect the triggering of the monitor signal in accordance with a predetermined numerical threshold and corresponding re-setting of the accumulator 44.

The monitor circuit 34 may be implemented using hardware logic. As such, a hardware implementation may provide a considerable improvement in economy of power, over a use of a microprocessor. Use of hardware to implement monitor circuit 34, instead of a microprocessor removes a limitation on a repetition frequency at which audible signals can be generated as a result of a microprocessor being powered up in accordance with a predetermined duty cycle. As a result of a hardware implementation, the monitor circuit 34, may be operated continuously in a power efficient manner thereby obviating any requirement for operation in accordance with a duty cycle, and so removing any limit on the repetition frequency of the audible signals.

As will be appreciated by those skilled in the art, various modifications may be made to the embodiments hereinbefore described without departing from the scope of the present invention. In particular, various other forms of shield may be constructed whilst still providing the combined radiological and electromagnetic shielding effects provided by the present invention. Furthermore, other means may be provided for generating the photons of light used to test the radiation detector other than a light emitting diode. Other means may also be used for effecting operation of the audio monitor signal in accordance with accumulating predetermined numbers representative of an affect of radiation particles detected by a corresponding radiation detector.

CLAIMS;

1. A personal radiation dosimeter comprising a radiation detector means coupled to an electronic measurement circuit and arranged in combination to generate signals representative of an amount of
5 radiation received by said radiation detector means, wherein there is further provided a shield arranged to be electrically coupled to an earth plane and to substantially surround a volume in which said radiation detector means is disposed, said shield being fabricated from electrically conductive material so as to provide substantial
10 electromagnetic screening, which electrically conductive material has a composition and density sufficiently high to provide substantial radiological shielding, for substantially low energy radiation particles, said shield being thereby arranged to provide both electromagnetic and radiological screening.
- 15 2. A personal radiation dosimeter as claimed in Claim 1, wherein said electrically conductive material is a metal.
3. A personal radiation dosimeter as claimed in Claim 2, wherein the metal is tin.

4. A personal radiation dosimeter as claimed in Claim 2, wherein said electrically conductive material is an alloy.
5. A personal radiation dosimeter as claimed in Claim 4, wherein
5 the alloy is pewter.
6. A personal radiation dosimeter comprising a radiation detector means coupled to an electronic measurement circuit arranged in combination therewith to generate signals representative of an amount of radiation detected by said radiation detector, wherein said radiation
10 detector means is provided with a light source optically coupled to said radiation detector means and arranged to operate under control of a test control circuit to generate light of a wavelength which may be detected by said radiation detector, thereby providing in combination with said electronic measurement circuit an integrity test for said radiation
15 detector means.
7. A personal radiation dosimeter as claimed in Claim 6, wherein the light source is a light emitting diode.

8. A personal radiation dosimeter as claimed in Claims 6 or 7,
wherein the optical coupling includes an optical fibre arranged to
convey the light to said radiation detector means.
- 5 9. A personal radiation dosimeter as claimed in Claims 6 or 7,
wherein the optical coupling is effected by reflection via a surface of
the shield.
10. A personal radiation dosimeter as claimed in any of Claims 6-9,
further including a screen which serves to shield said radiation detector
10 from ambient light.
11. A personal radiation dosimeter for generating a monitor signal
representative of a radiation dose rate, said radiation dosimeter
comprising a radiation detector means coupled to an electronic
measurement circuit and arranged in combination therewith to generate
15 signals representative of an amount of radiation received by said
radiation detector, wherein said electronic measurement circuit includes
at least one data store, an accumulator means and control circuit means,
which control circuit means is coupled to said radiation detector means
and arranged to add a predetermined number stored in said data store to

an accumulated total stored in said accumulator in response to signals from said radiation detector means, said control circuit being arranged to generate a monitor signal for each increment of said accumulated
5 total by said predetermined numerical threshold, which monitor signal is fed to an audio signal generator so as to provide an audible signal in accordance with said increment, a repetition frequency of said audible signal being thereby representative of said radiation dose rate.

12. A personal radiation dosimeter as claimed in Claim 11, further
10 comprising at least one other radiation detector means and at least one other data store, wherein said at least one other data store includes a further predetermined number and said control circuit operates to add said further predetermined number to said accumulator consequent upon receipt of signals from said at least one other radiation detector
15 means.

13. A personal radiation dosimeter as claimed in Claim 12, wherein said first and said further predetermined numbers are selected in combination with the numerical threshold, so that the radiation

dosemeter is arranged to generate a monitor signal at a frequency which is arranged to provide an audible indication determined by the relative harm caused by the radiation detected by the first and further radiation
5 detector means.

14. A personal radiation dosimeter as claimed in any of Claims 10-12, wherein said predetermined numerical threshold is representative of a maximum count which is available to said accumulator, and said monitor signal is generated from an overflow signal generated by the
10 accumulator.

15. A method of generating a monitor signal representative of a radiation dose rate, said method comprising the steps of:

adding said predetermined number to an accumulated total upon receipt of a first signal from a first radiation detector,

15 comparing said accumulated total with a predetermined numerical threshold and

generating a monitor signal if the accumulated total has changed since a last monitor signal was generated by said predetermined numerical threshold.

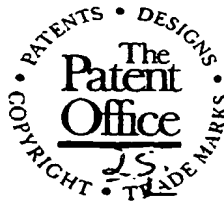
- 5 16. A method of generating a monitor signal as claimed in Claim 15, further including the steps of

adding said further predetermined number to said accumulated total upon receipt of a further signal from a further radiation detector.

17. A personal radiation dosimeter as hereinbefore described with
10 reference to Figure 1, 2, 3 and 4.

Amendments to the claims have been filed as follows**CLAIMS:**

1. A personal radiation dosimeter comprising a radiation detector means coupled to
5 an electronic measurement circuit and arranged in combination to generate signals
representative of an amount of radiation received by said radiation detector means,
wherein there is further provided a shield arranged to be electrically coupled to an
earth plane and to substantially surround a volume in which said radiation detector
10 means is disposed, said shield being fabricated from electrically conductive
material so as to provide substantial electromagnetic screening, which electrically
conductive material has a composition and density sufficiently high to provide
substantial radiological shielding, for substantially low energy radiation particles,
said shield being thereby arranged to provide both electromagnetic and radiological
15 screening.
2. A personal radiation dosimeter as claimed in Claim 1, wherein said electrically
conductive material is a metal.
3. A personal radiation dosimeter as claimed in Claim 2, wherein the metal is tin.
20
4. A personal radiation dosimeter as claimed in Claims 2, wherein said electrically
conductive material is an alloy.
5. A personal radiation dosimeter as claimed 4, wherein the alloy is pewter.
25
6. A personal radiation dosimeter as hereinbefore described with reference to Fig. 1.



INVESTOR IN PEOPLE

Application No: GB 0123075.4
Claims searched: 1-5

Examiner: W Euros Morris
Date of search: 23 October 2001

Patents Act 1977 Search Report under Section 17

Databases searched:

UK Patent Office collections, including GB, EP, WO & US patent specifications, in:

UK Cl (Ed.S): G1A (AFE, AHLR, ART)

Int Cl (Ed.7): G01T: 1/00, 1/02, 1/14, 1/16, 1/40

Other: Online: WPI, EPODOC, JAPIO

Documents considered to be relevant:

Category	Identity of document and relevant passage	Relevant to claims
A	GB 2254692 A (GENERAL ELECTRIC COMPANY)	

N	Document indicating lack of novelty or inventive step	A	Document indicating technological background and/or state of the art.
Y	Document indicating lack of inventive step if combined with one or more other documents of same category.	P	Document published on or after the declared priority date but before the filing date of this invention.
&	Member of the same patent family	E	Patent document published on or after, but with priority date earlier than, the filing date of this application.